

Joint Reconstruction of Phase-Cycled Balanced SSFP with Constrained Parallel Imaging

B Bilgic^{1,2}, T Witzel^{1,2}, H Bhat³, LL Wald^{1,2}, K Setsompop^{1,2}

1 Martinos Center, Charlestown, MA, USA

2 Harvard Medical School, Boston, MA, USA

3 Siemens Medical Solutions, Charlestown, MA, United States

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Declaration of Financial Interests or Relationships

Speaker Name: Berkin Bilgic

I have the following financial interest or relationship(s) to disclose with regard to the subject matter of this presentation:

- Research support: Siemens
- Licensing agreement: Samsung

Balanced SSFP

- bSSFP has
 - unique T2 / T1 contrast
 - inherent high SNR efficiency
 - fast imaging time: short TE & TR
- Provides strong contrast between tissues with different T2 / T1 ratios
 - ❖ Cardiac [1] (blood – myocardium contrast)
 - ❖ Angio [2] (blood – surrounding tissue)
 - ❖ MSK [3] (fat – muscle)
 - ❖ Neuro [4] nerves at skull base (CSF – cranial nerve)

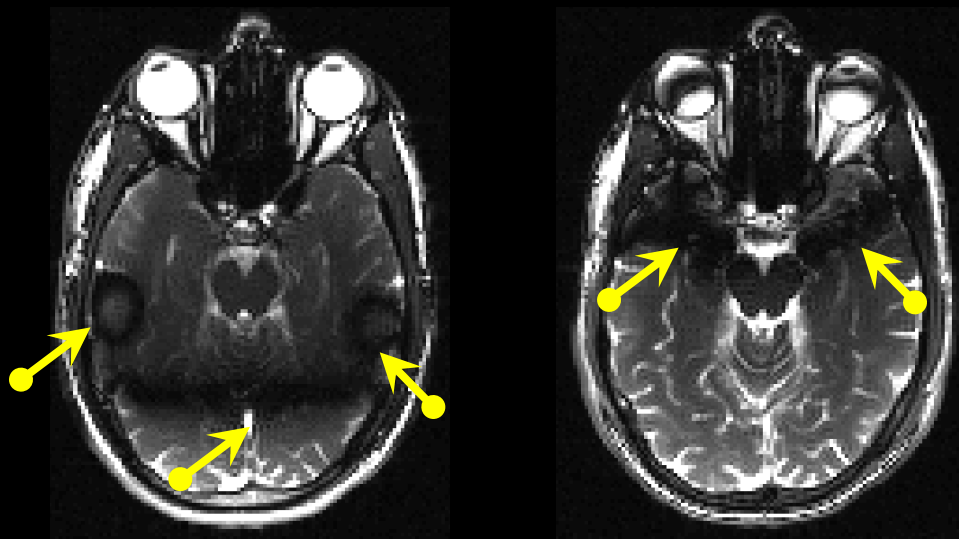
[1] DC Peters et al MRM 2002

[2] NK Bangerter et al MRM 2011

[3] GE Gold et al JMRI 2007

[4] JW Casselman et al Am Soc Neuroradiology 1993

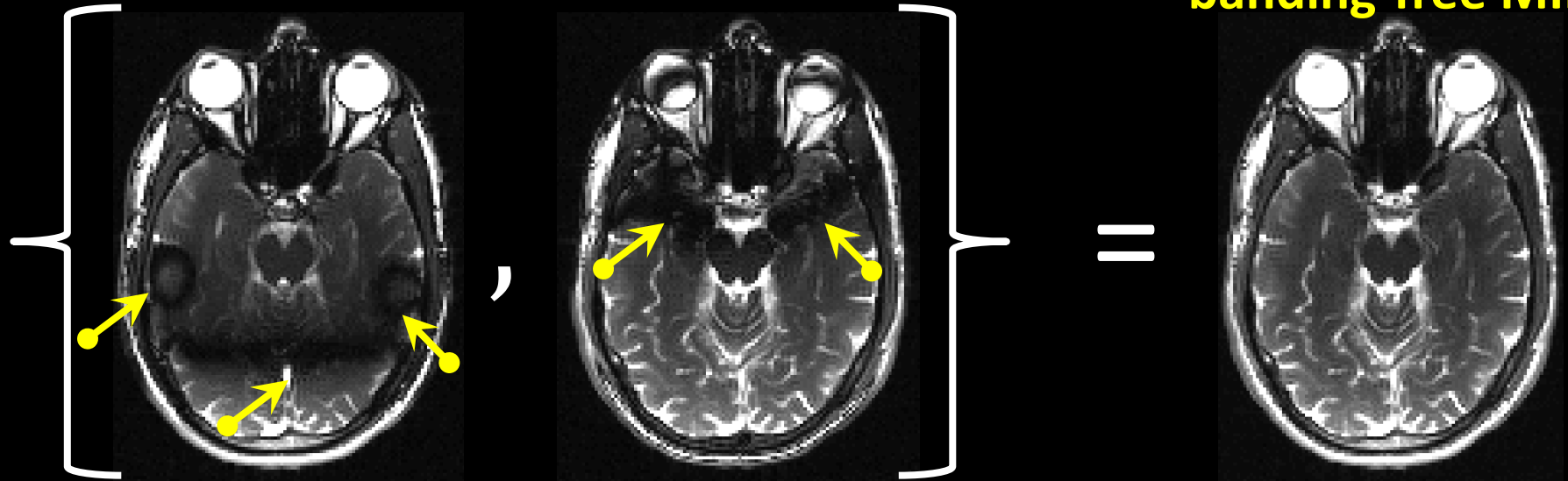
Phase-cycled bSSFP



- But suffers from banding artifacts due to sensitivity to B0 inhomogeneity
- Can be mitigated by phase-cycling:
 - ❖ multiple acquisitions with different phase increment btw successive RFs
 - ❖ this shifts location of banding artifacts

Phase-cycled bSSFP

max



- But suffers from banding artifacts due to sensitivity to B0 inhomogeneity
- Can be mitigated by phase-cycling:
 - ❖ multiple acquisitions with different phase increment btw successive RFs
 - ❖ this shifts location of banding artifacts
 - ❖ combine cycles with Max Intensity Projection (MIP)

Phase-cycled bSSFP

- Phase-cycling mitigates banding artifacts
- But increases scan time, counteracting inherent efficiency of bSSFP

- Parallel Imaging [1,2] and Simultaneous MultiSlice (SMS) [3,4] employ receiver sensitivity encoding to reduce scan time
- And have been deployed in phase-cycled bSSFP for up to 4-fold acceleration [5,6]

[1] KP Pruessmann et al MRM 1999

[2] MA Griswold et al MRM 2002

[3] DJ Larkman et al JMRI 2001

[4] FA Breuer et al MRM 2005

[5] D Stab et al MRM 2011

[6] Y Wang et al MRM 2015

Joint Recon for Phase-cycled bSSFP

- We propose to jointly recon phase-cycled images
- We introduce **Joint L1-SPIRiT**:
 - ❖ recons all phase-cycles simultaneously to exploit their mutual info
 - ❖ fit SPIRiT kernels [1] jointly across coils and phase-cycles
 - ❖ analogous to k - t in dynamic imaging [2], *virtual coil* in diffusion imaging [3] and joint recon in TIAMO [4]

[1] M Lustig et al MRM 2010

[2] F Huang et al MRM 2005

[3] E Dai et al MRM 2016

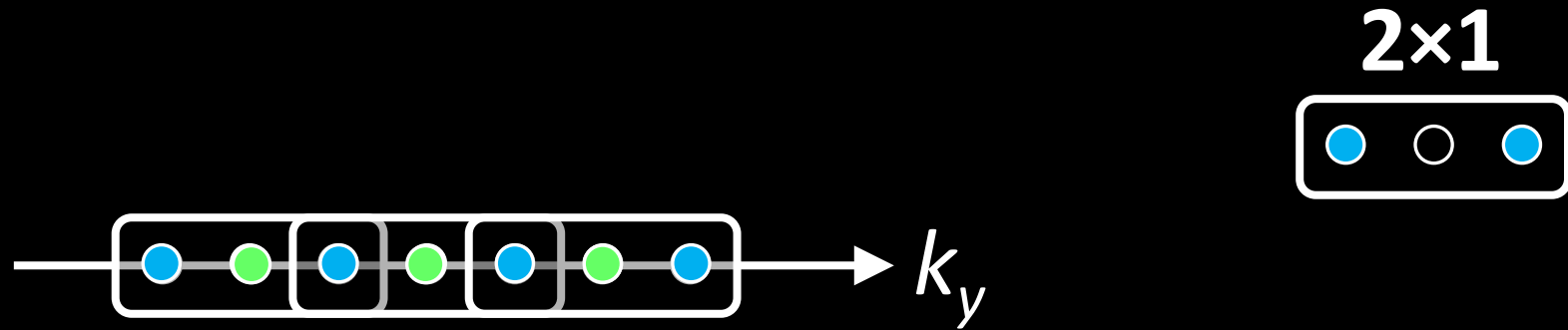
[4] S Orzada et al MRM 2010

Joint Recon for Phase-cycled bSSFP

- We propose to jointly recon phase-cycled images
- We introduce Joint L1-SPIRiT:
 - ❖ by creating virtual coils out of the phase-cycles,
converts banding artifacts into useful, additional spatial encoding
 - ❖ reduction in g-factor noise amplification is > 1.8 -fold relative to GRAPPA
SNR improvement is similar to 3 averages of GRAPPA recon

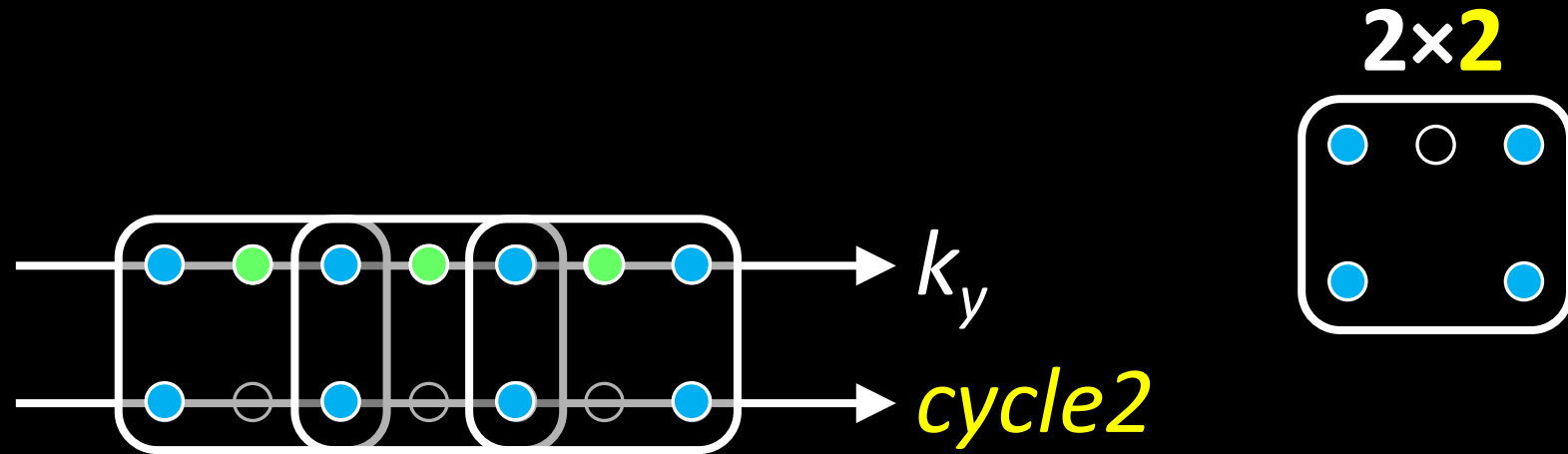
GRAPPA Recon

- R=2 acceleration, ignoring coil and readout axes



Joint GRAPPA

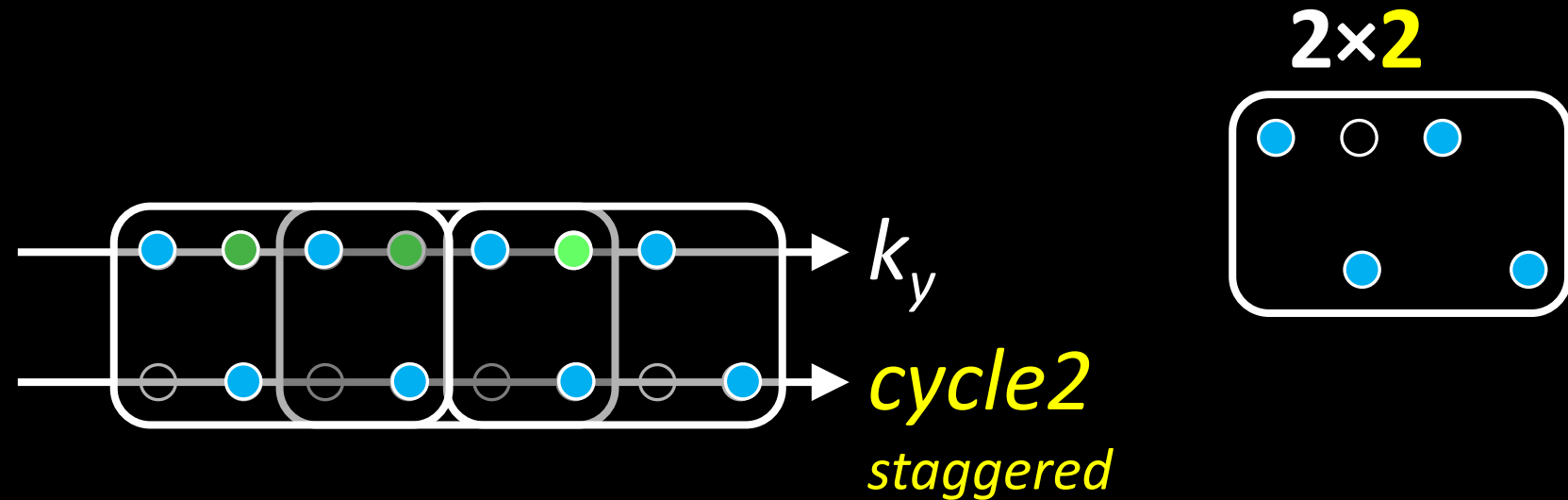
- Extend GRAPPA to jointly recon all phase-cycles [1]



[1] B Bilgic et al ESMRMB'16

Joint GRAPPA

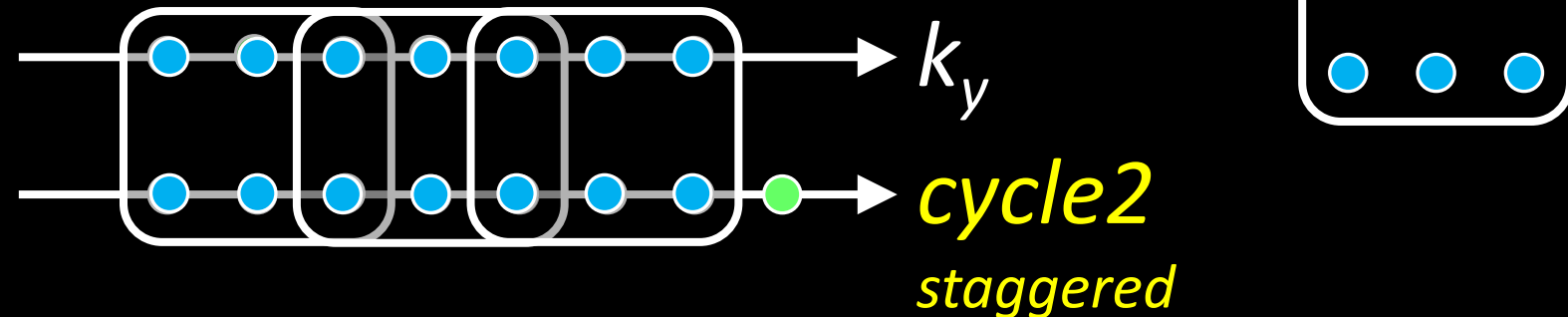
- Staggered sampling for complementary k-space info:



[1] B Bilgic et al ESMRMB'16

Proposed: Joint L1-SPIRiT

- Staggered sampling for complementary k-space info:
- SPIRiT uses compact kernels and permits L1 regularization



+ Total Variation regularization

Data Reconstruction

- GCC coil compression to 12 channels [1]
- Kernels estimated with Tikhonov regularization from 32 ACS lines
- Regularization, kernel sizes and staggering amount optimized for best RMSE
- G-factor from 300 Monte-Carlo iterations [2]

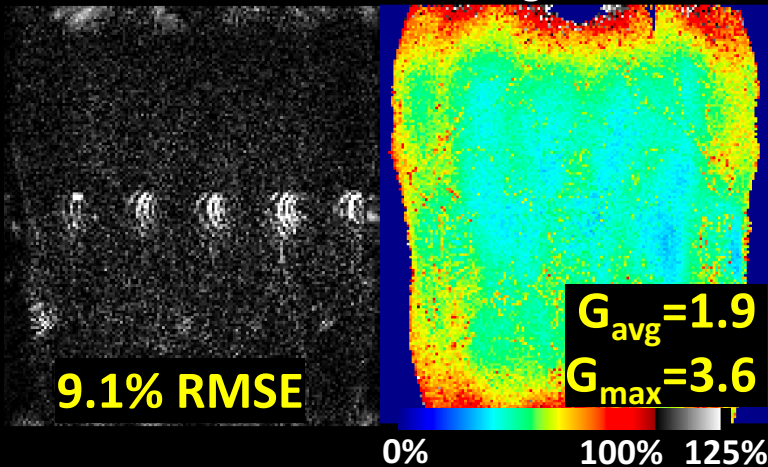
Abdominal 2D bSSFP acquisition
four phase-cycles, acceleration R=6

GRAPPA



Error scaled 5×

1/g-factor



- ❖ four cycles $\{0, \pi/2, \pi, 3\pi/2\}$
- ❖ FOV = $380 \times 380 \text{ mm}^2$,
- ❖ 5 mm thick slice
- ❖ mtx = 160×160
- ❖ TR/TE = 3.3/1.54 ms
- ❖ 34-chan

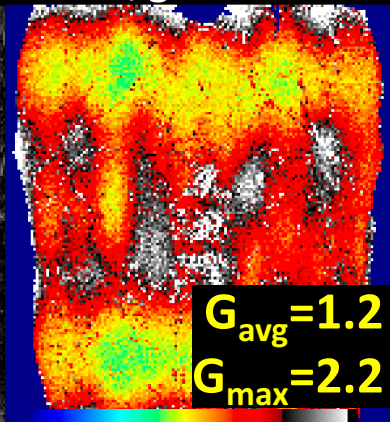
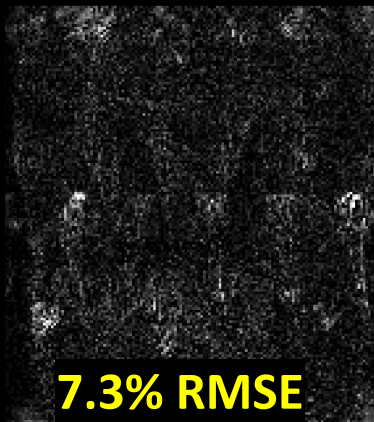
Abdominal 2D bSSFP acquisition
four phase-cycles, acceleration R=6

Joint GRAPPA



Error scaled 5×

1/g-factor



7.3% RMSE

$G_{avg}=1.2$

$G_{max}=2.2$

0% 100% 125%

- ❖ four cycles $\{0, \pi/2, \pi, 3\pi/2\}$
- ❖ FOV = $380 \times 380 \text{ mm}^2$,
- ❖ 5 mm thick slice
- ❖ $mtx = 160 \times 160$
- ❖ TR/TE = 3.3/1.54 ms
- ❖ 34-chan

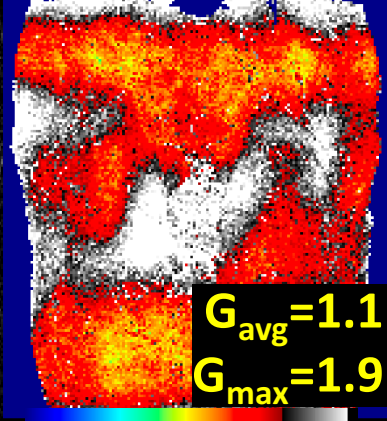
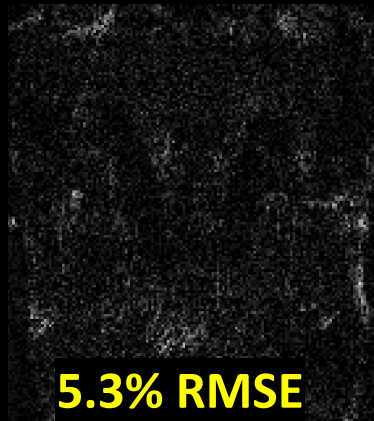
Abdominal 2D bSSFP acquisition
four phase-cycles, acceleration R=6

**Proposed:
Joint L1-SPIRiT**



Error scaled 5×

1/g-factor



0% 100% 125%

- ❖ four cycles $\{0, \pi/2, \pi, 3\pi/2\}$
- ❖ FOV = 380×380 mm²,
- ❖ 5 mm thick slice
- ❖ mtx = 160×160
- ❖ TR/TE = 3.3/1.54 ms
- ❖ 34-chan

Abdominal 2D bSSFP acquisition
four phase-cycles, acceleration R=6

**Proposed:
Joint L1-SPIRiT**



RMSE reduced 70%

G_{\max} reduced 1.9-fold

G_{avg} reduced 1.7-fold

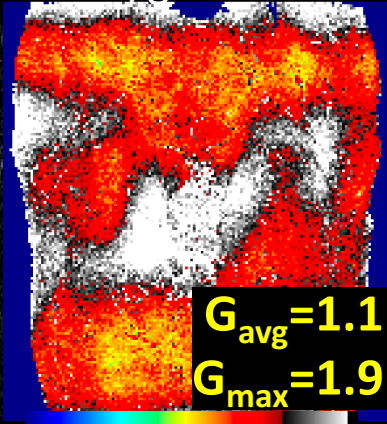
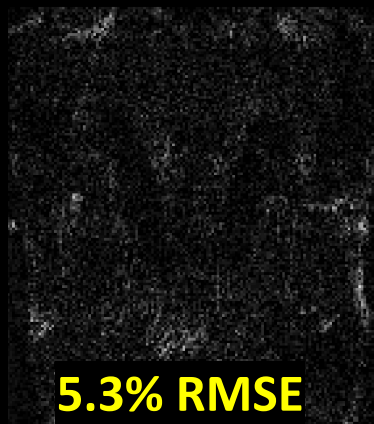
**SNR improvement is
~3 averages of GRAPPA**

GRAPPA



Error scaled 5×

1/g-factor



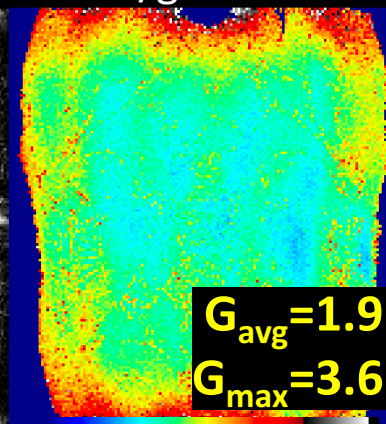
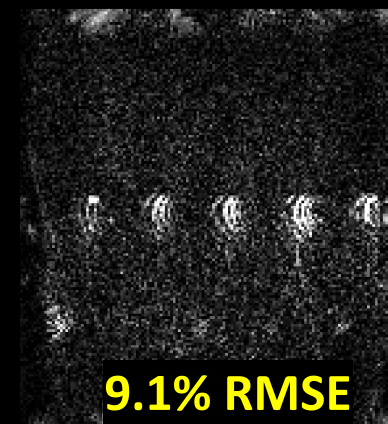
$G_{\text{avg}}=1.1$

$G_{\max}=1.9$

0% 100% 125%

Error scaled 5×

1/g-factor



$G_{\text{avg}}=1.9$

$G_{\max}=3.6$

0% 100% 125%

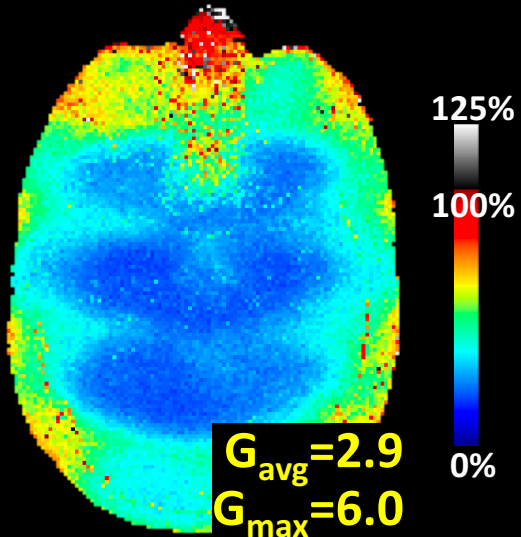
Neuro 2D bSSFP acquisition
four phase-cycles, acceleration R=6

GRAPPA



10.0%
RMSE

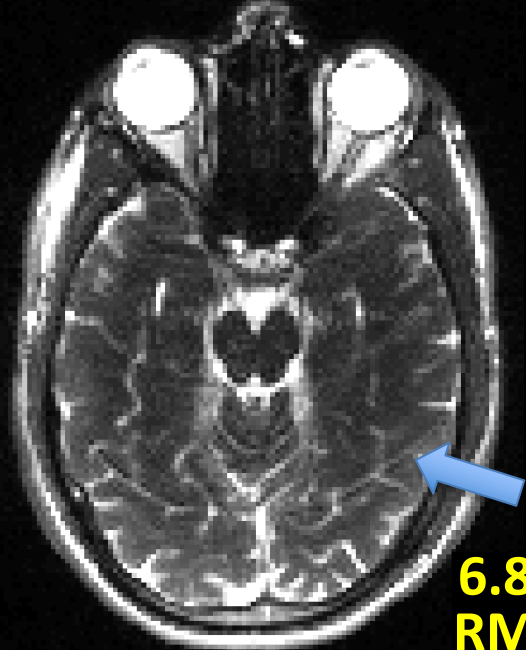
1/g-factor



- ❖ four cycles $\{0, \pi/2, \pi, 3\pi/2\}$
- ❖ FOV = 240×240 mm²,
- ❖ 4.5 mm thick slice
- ❖ mtx = 160×160
- ❖ TR/TE = 3.4/1.6 ms
- ❖ 32-chan

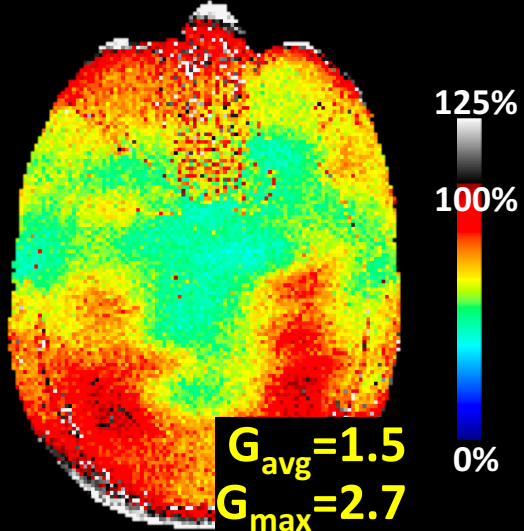
Neuro 2D bSSFP acquisition
four phase-cycles, acceleration R=6

Joint GRAPPA



6.8%
RMSE

1/g-factor



- ❖ four cycles $\{0, \pi/2, \pi, 3\pi/2\}$
- ❖ FOV = $240 \times 240 \text{ mm}^2$,
- ❖ 4.5 mm thick slice
- ❖ $\text{mtx} = 160 \times 160$
- ❖ TR/TE = 3.4/1.6 ms
- ❖ 32-chan

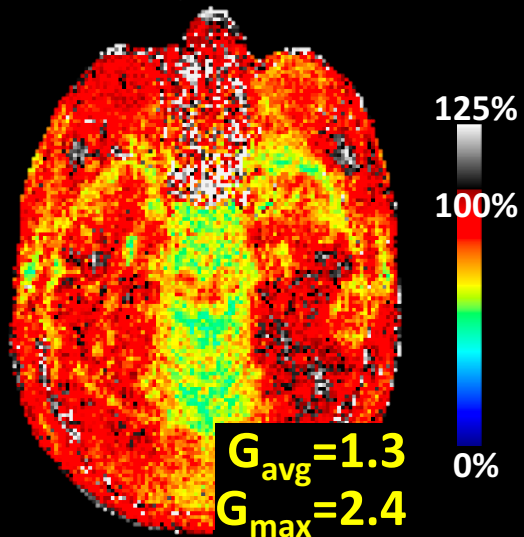
Neuro 2D bSSFP acquisition
four phase-cycles, acceleration R=6

Proposed: Joint L1-SPIRiT



5.2%
RMSE

1/g-factor



- ❖ four cycles $\{0, \pi/2, \pi, 3\pi/2\}$
- ❖ FOV = 240×240 mm²,
- ❖ 4.5 mm thick slice
- ❖ mtx = 160×160
- ❖ TR/TE = 3.4/1.6 ms
- ❖ 32-chan

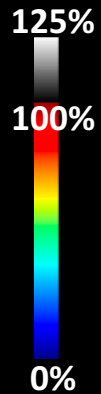
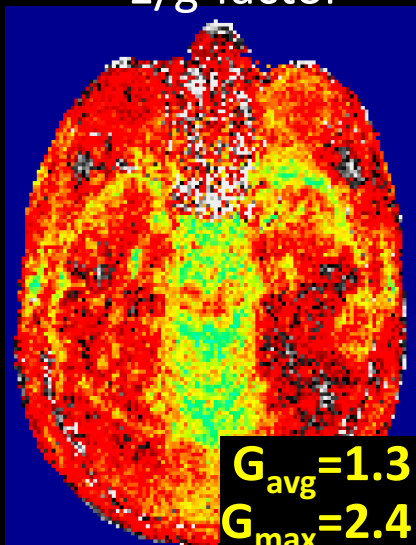
Neuro 2D bSSFP acquisition
four phase-cycles, acceleration R=6

Proposed: Joint L1-SPIRiT



5.2%
RMSE

1/g-factor



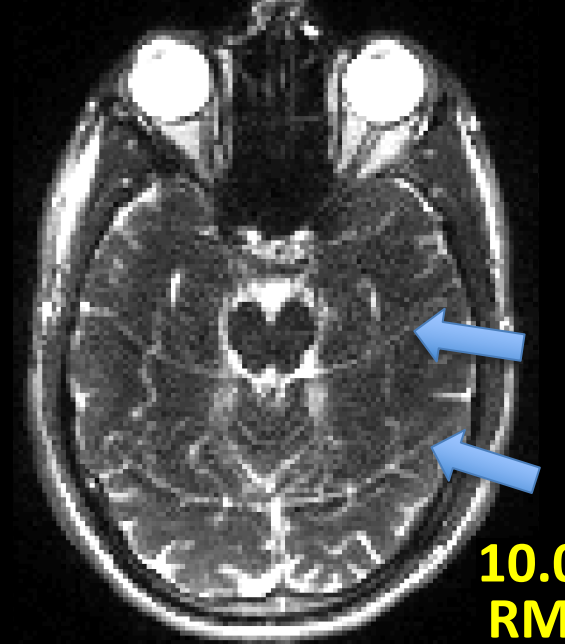
RMSE reduced 90%

G_{max} reduced 2.5-fold

G_{avg} reduced 2.2-fold

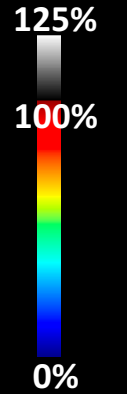
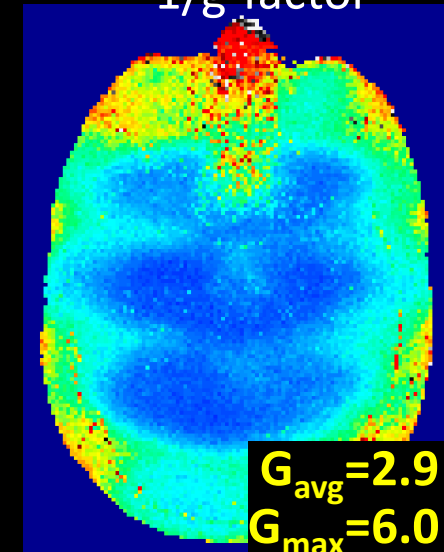
SNR improvement is
>4 averages of GRAPPA

GRAPPA



10.0%
RMSE

1/g-factor



Neuro 2D bSSFP acquisition
four phase-cycles, acceleration R=6

Proposed: Joint L1-SPIRiT

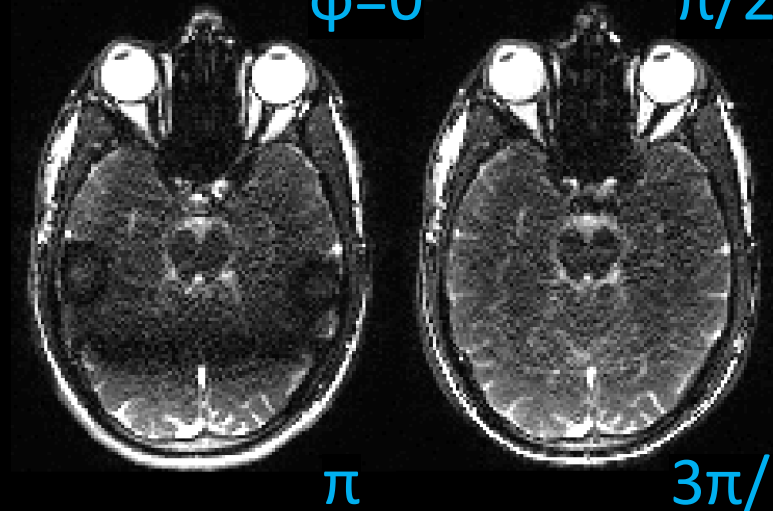
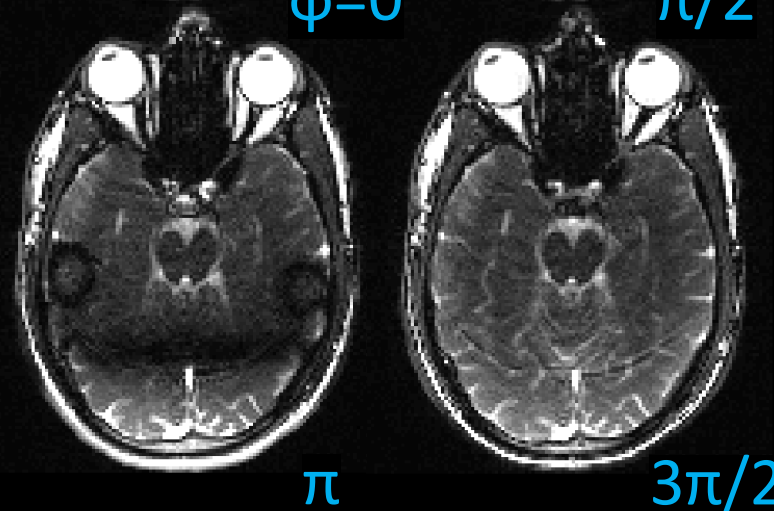
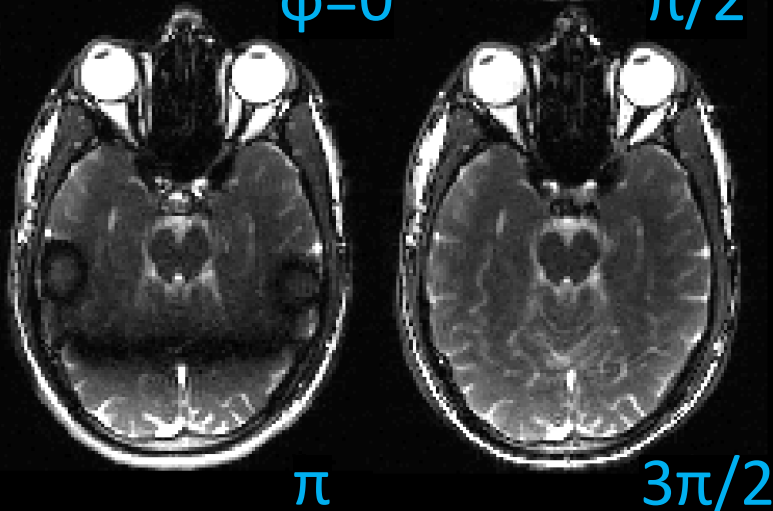
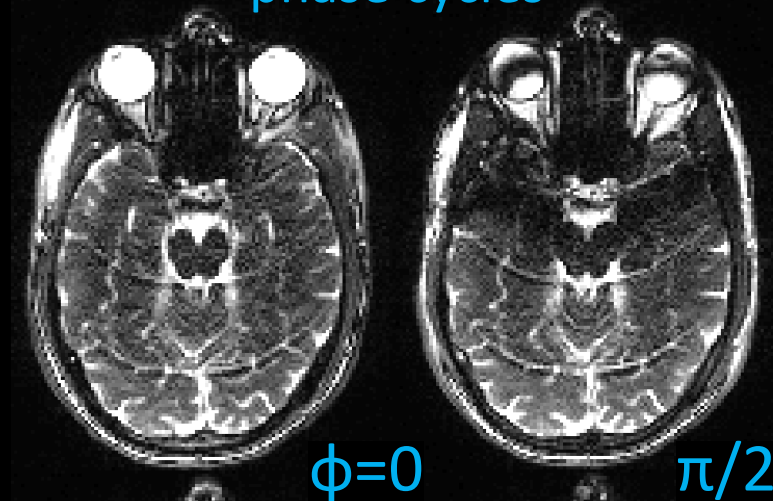
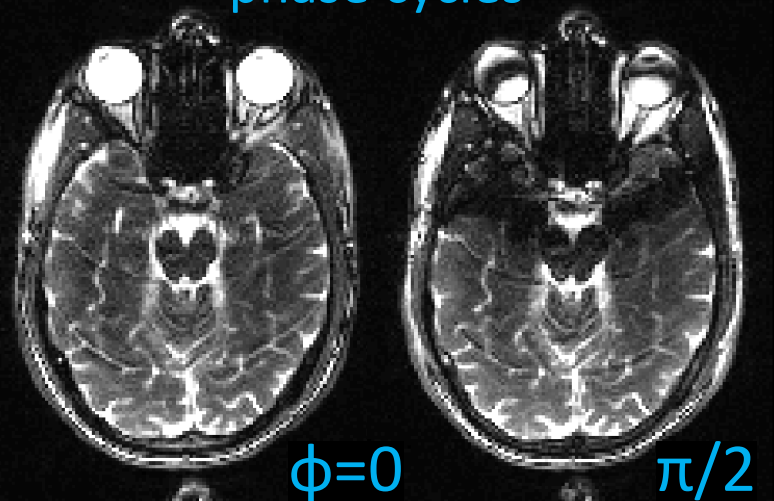
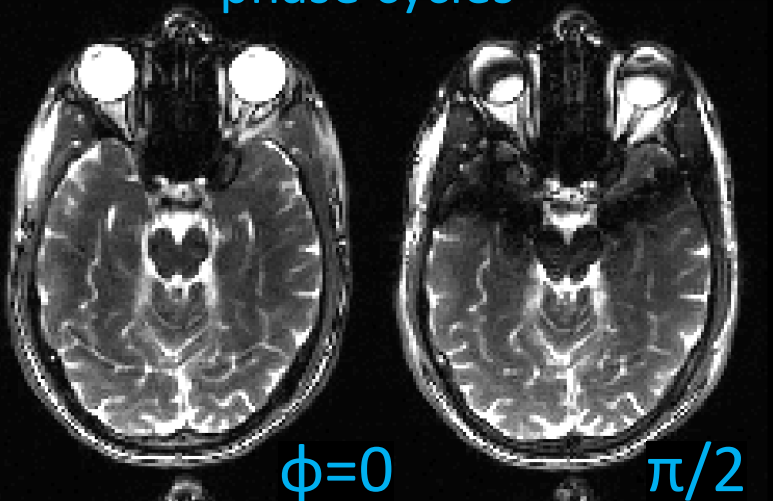
Joint GRAPPA

GRAPPA

phase cycles

phase cycles

phase cycles



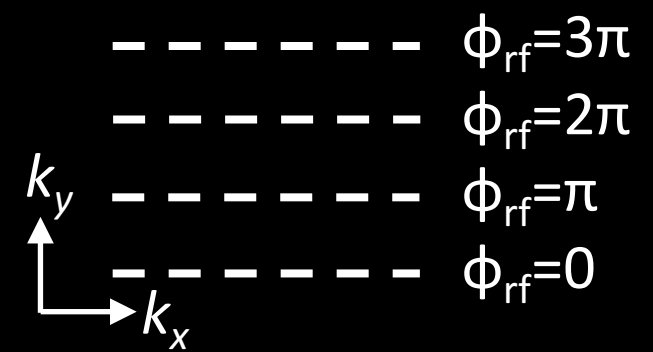
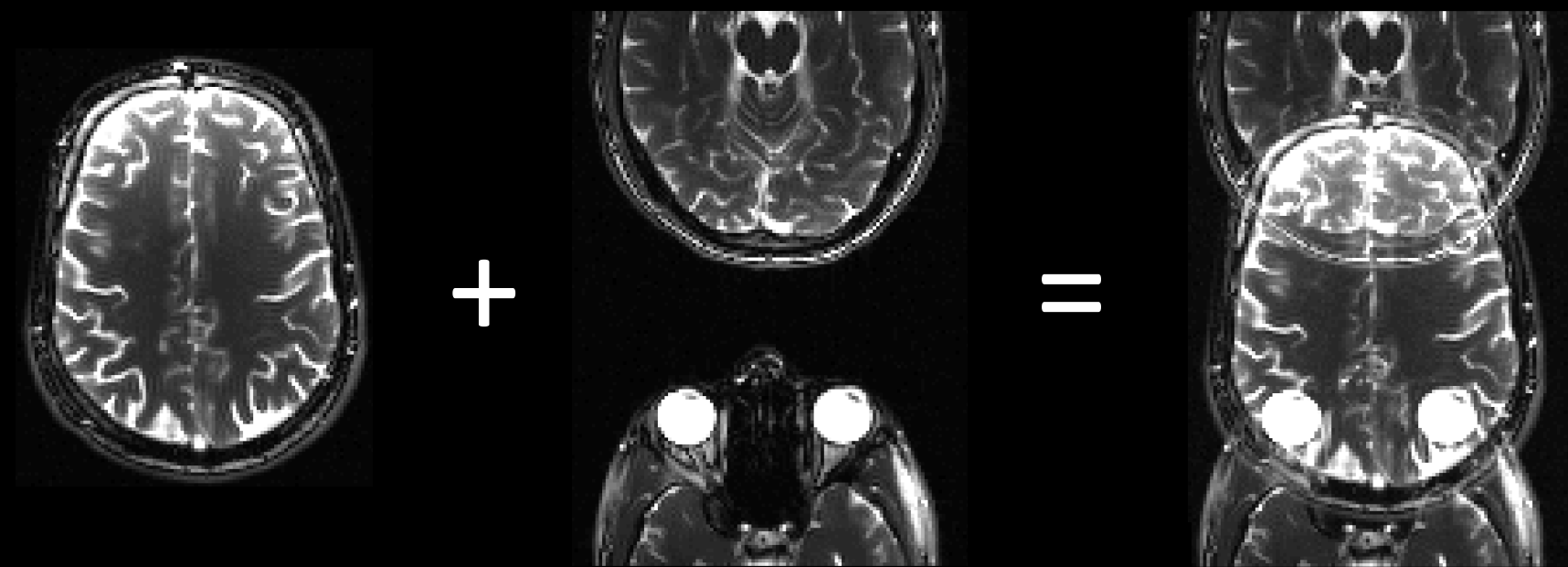
Simultaneous MultiSlice bSSFP

- SMS: simultaneously excite and encode multiple slices



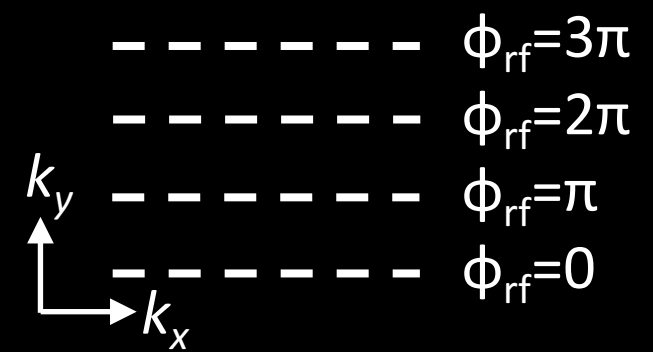
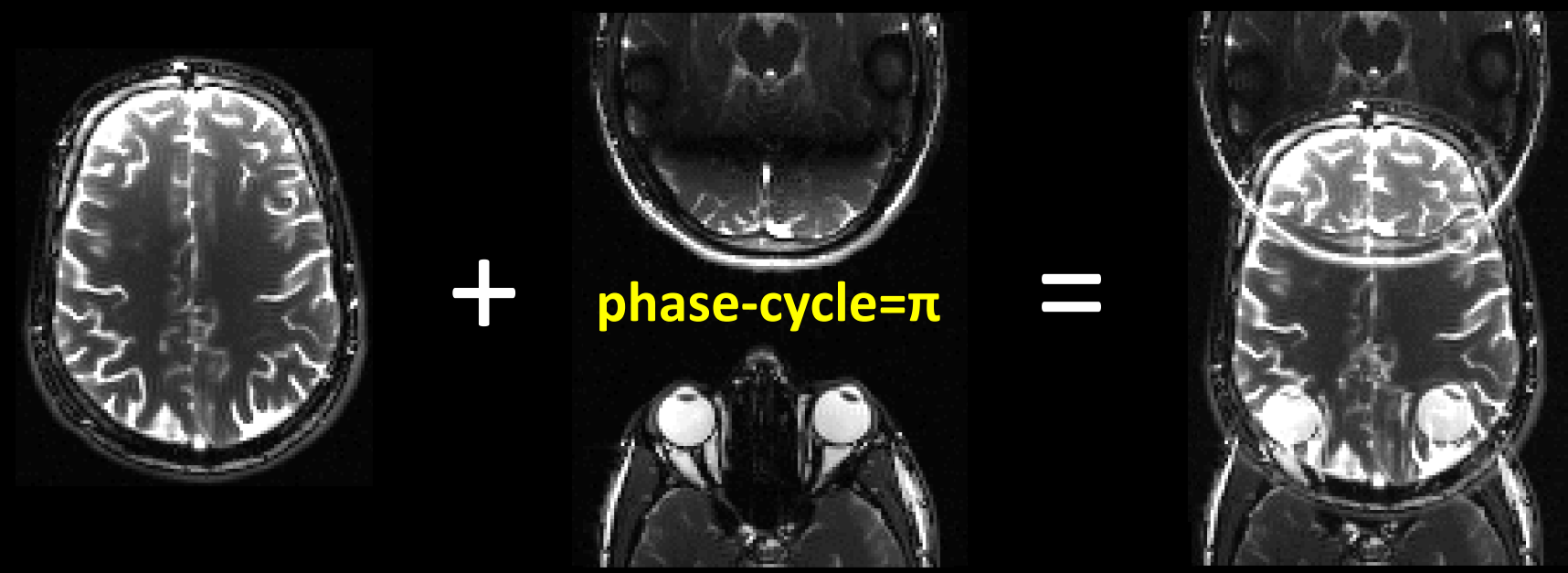
Simultaneous MultiSlice bSSFP

- SMS: simultaneously excite and encode multiple slices
- Incur FOV shift across slices to improve parallel imaging



Simultaneous MultiSlice bSSFP

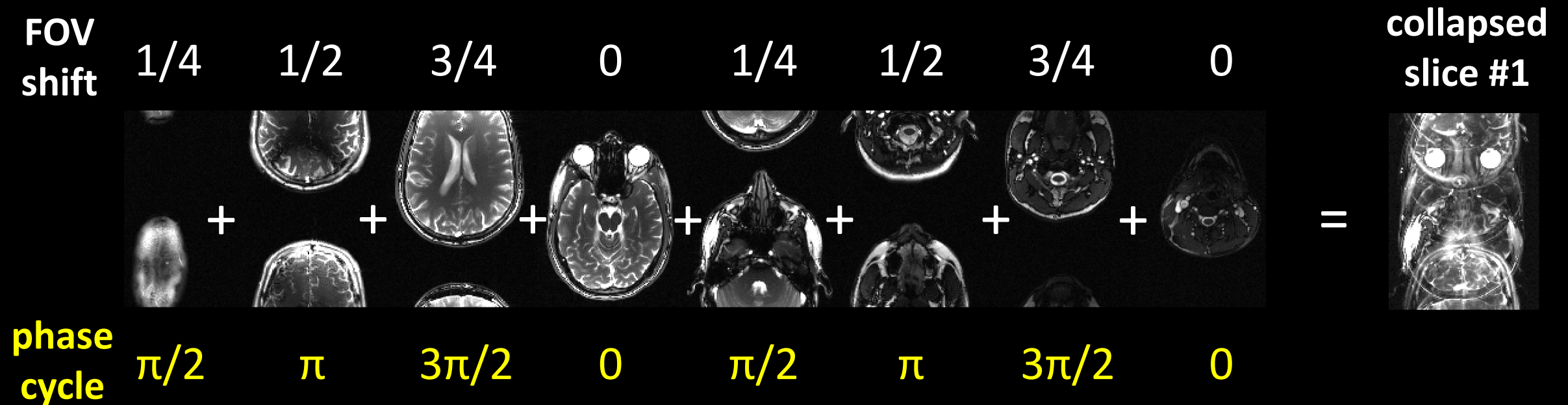
- SMS: simultaneously excite and encode multiple slices
- Incur FOV shift across slices to improve parallel imaging



FOV/2 slice shift also causes off-resonance shift by π

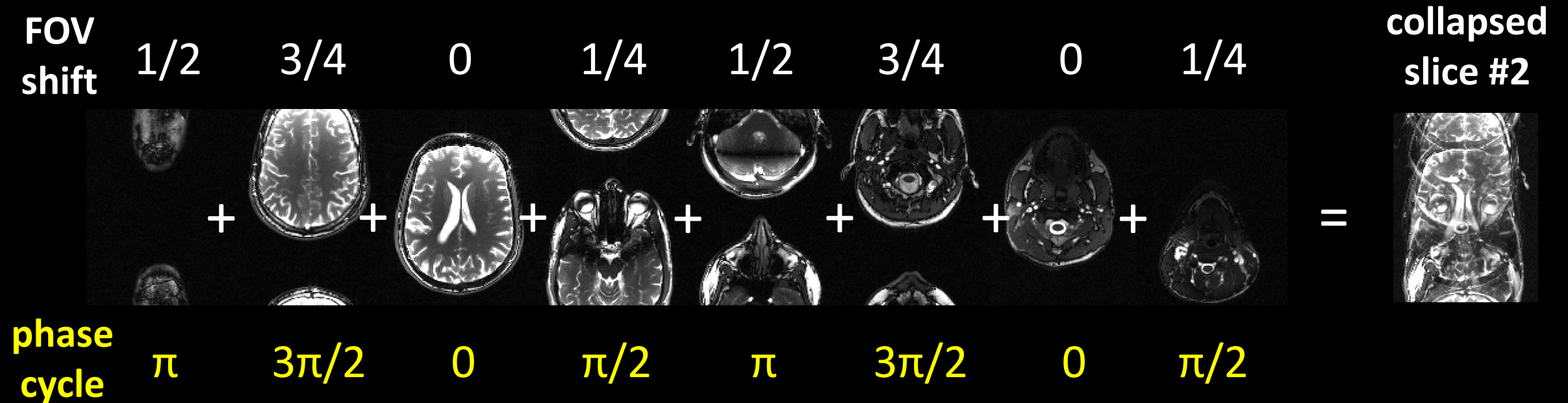
Simultaneous MultiSlice bSSFP @ MultiBand=8

- At MultiBand=8, each collapsed slice has contribution from four phase-cycles:



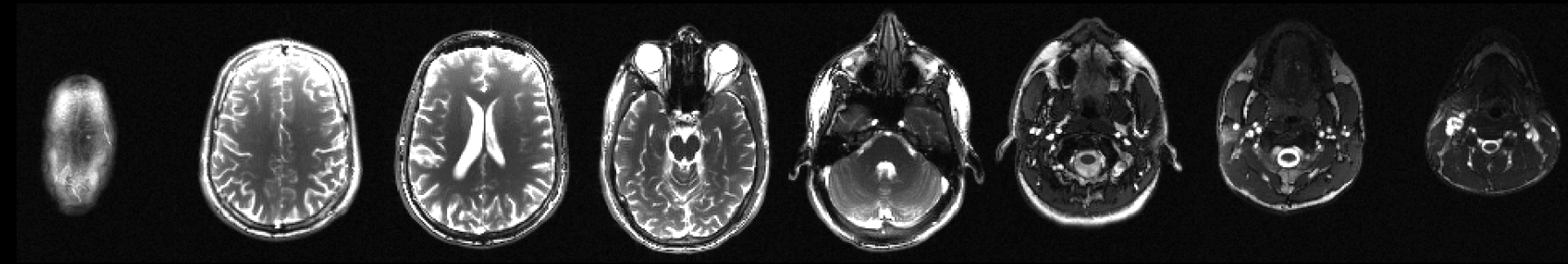
Simultaneous MultiSlice bSSFP @ MultiBand=8

- At MultiBand=8, each collapsed slice has contribution from four phase-cycles:



Simultaneous MultiSlice bSSFP @ MultiBand=8

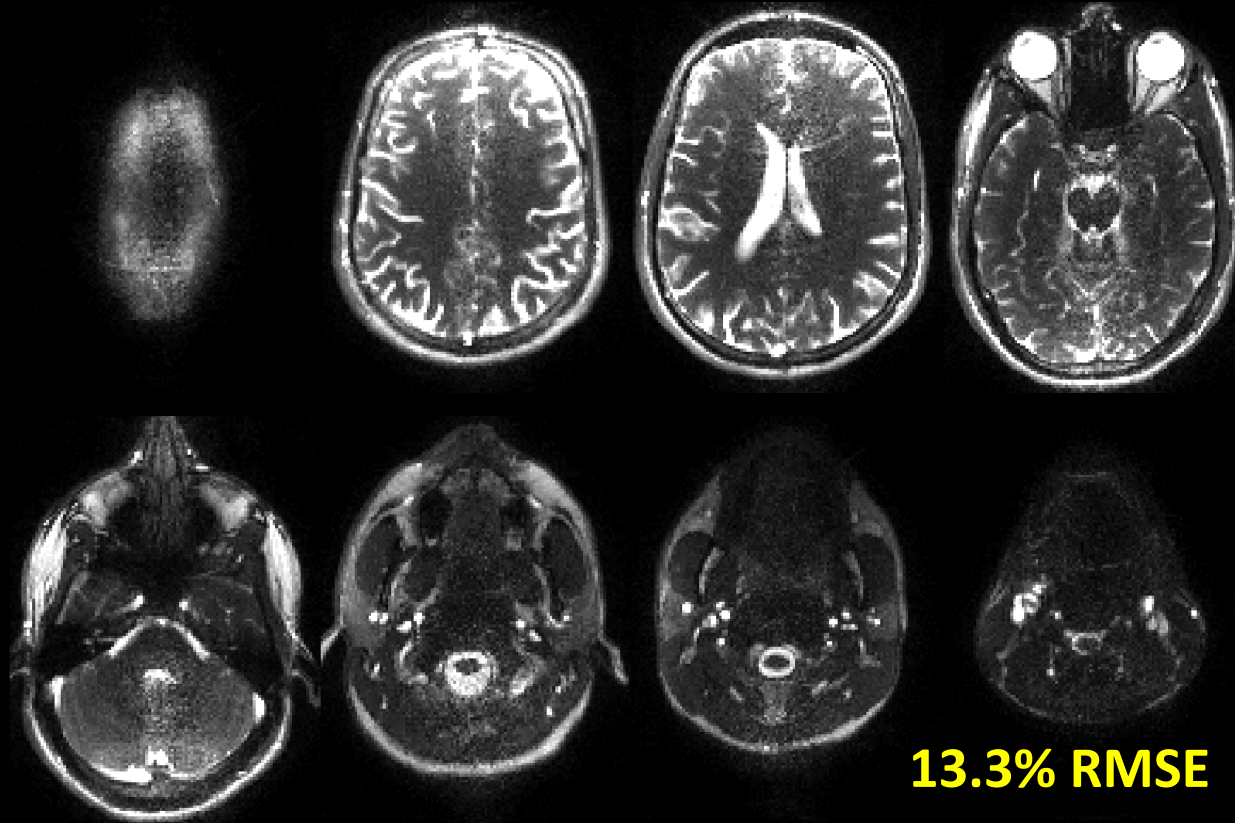
- At MultiBand=8, each collapsed slice has contribution from four phase-cycles
- After unaliasing collapsed slices and shifting slices back, apply MIP combination:



MIP combination

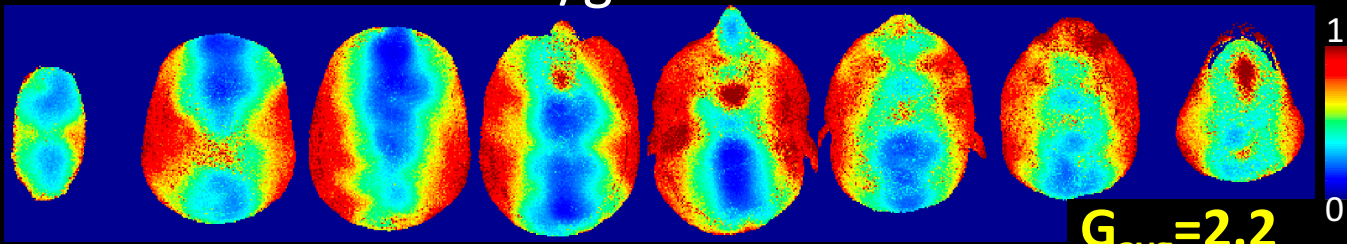
Neuro SMS acquisition
four cycles, MultiBand = 8

Split Slice GRAPPA



13.3% RMSE

1/g-factor

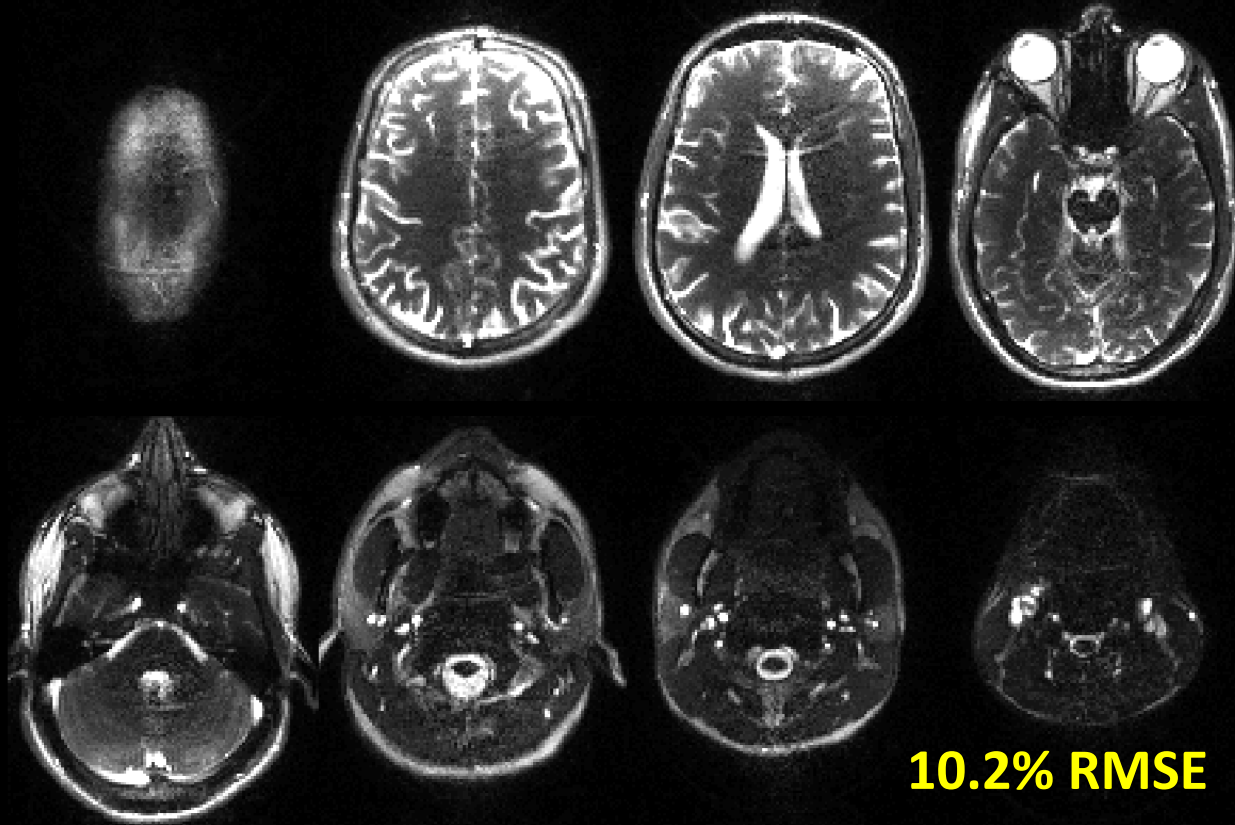


$G_{avg}=2.2$
 $G_{max}=11.3$

- ❖ 8 slices acquired separately
- ❖ Collapsed retrospectively
- ❖ FOV/4 slice shift

Neuro SMS acquisition
four cycles, MultiBand = 8

Joint Slice GRAPPA



RMSE reduced 30%

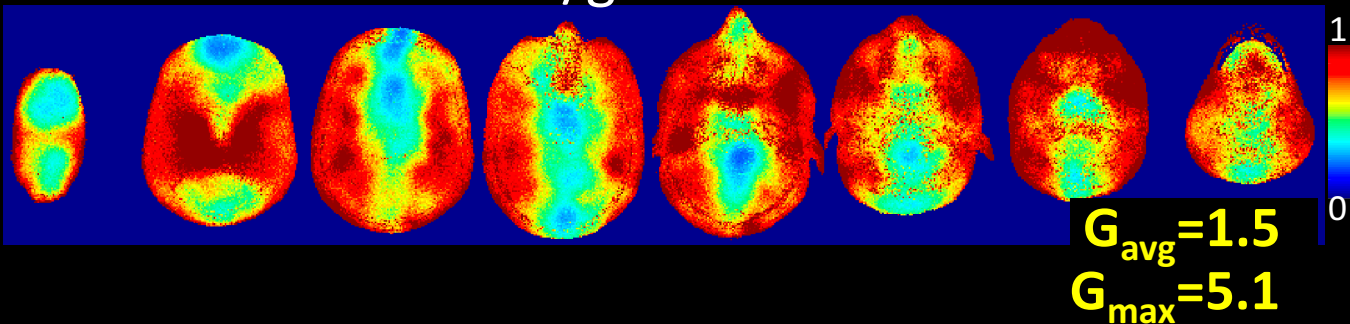
G_{\max} reduced 2.2-fold

G_{avg} reduced 1.5-fold

**SNR improvement is
>2 averages of GRAPPA**

10.2% RMSE

1/g-factor



Conclusion

- Joint L1-SPIRiT improves parallel imaging for phase-cycled bSSFP, with substantial reduction in noise amplification and recon error
- This allows high acceleration to mitigate scan time burden of phase-cycling
- **Limitations include:**
 - ❖ Cycles need to be registered for joint recon → gating, breath-hold
 - ❖ No of kernels scale with (no of cycles)² → smaller no of GCC channels

Thanks!

Questions / Comments:

berkin@nmr.mgh.harvard.edu

martinos.org/~berkin

Support: NIH

R24 MH106096

R01 EB020613

R01 EB017337

U01 HD087211